

## A mathematical approach to mitral regurgitation

### Mitral regurjitasyona matematiksel bir yaklaşım

Left ventricular end-diastolic pressure, left atrial pressure (LAP) and pulmonary capillary wedge pressure has been the subject of many investigations. The reason is that these pressures provide a good guide to assess the heart failure. Echocardiography is the method of choice in many instances. Evaluation of left ventricular pressure (LVP) may help in echocardiographic analysis of left ventricular filling pressures.

The mitral regurgitation (MR) can be detected by echocardiography with nearly 100% sensitivity (1). The MR is a good guide to assess left ventricular pressure. The Doppler recording of MR (MR jet) depends on the pressure gradient between left ventricle and left atrium, because it is this gradient that pushes the blood from left ventricle to left atrium. The relation has been described as (2):

$$\Delta P = \frac{1}{2}\delta(V_2^2 - V_1^2) + \delta(dV/dt)^*ds + R(\mu) \quad (\text{Eq. 1})$$

where  $\Delta P$  is the pressure difference across the stenosis,  $V_1$  and  $V_2$  are the velocities proximal and distal to the stenosis, respectively,  $\delta$  is the mass density of the blood,  $R$  is viscous resistance and  $\mu$  is viscosity. The last two terms are negligible; therefore, the Eq-1 converts to:

$$\Delta P = 4(V_2^2 - V_1^2) \quad (\text{Eq. 2})$$

In cases of very low  $V_1$ , the equation may finally be converted to:

$$\Delta P = 4V_2^2 \quad (\text{Eq. 3})$$

The MR jet is in fact a graphic of blood velocity versus time. Using the relation between  $\Delta P$  and blood velocity, we can rewrite the Eq. 3 as:

$$\Delta P/4 = V^2 \quad (\text{Eq. 4})$$

We know that:

$$\Delta P = LVP - LAP \quad (\text{Eq. 5})$$

where  $LVP$  is the left ventricular pressure and  $LAP$  is the left atrial pressure. Then,

$$LVP = \Delta P + LAP \quad (\text{Eq. 6})$$

During ventricular systole, change in  $LVP$  is much more prominent than change in  $LAP$ , with the exceptions of presence of V-wave. With this assumption, it can be concluded that the MR jet is also a reflection of  $LVP$ .

Although the entire time course of  $LVP$  cannot be converted to certain equations because of the variability in aortic properties, some equations have been proposed for isovolumic contraction and isovolumic relaxation phases, which are the periods that the aortic valve is not open, and therefore, aortic pressure is not equal to the left ventricular pressure. The mostly accepted example of such an equation is Weiss' formula which was suggested for defining left ventricular pressure during isovolumic relaxation phase (3):

$$P = P_0 \times e^{-t/\tau} \quad (\text{Eq. 7})$$

where the  $P$  is the instant pressure during isovolumic relaxation phase,  $P_0$  is the left ventricular pressure at any time before the time of left ventricular pressure of  $P$ ,  $e$  is the base of natural logarithm,  $t$  is the time interval between the pressure of  $P_0$  and  $P$ ,  $\tau$  is the isovolumic relaxation time constant.

Actually,  $P$  is equal to  $\Delta P + LAP$  and  $P_0$  is equal to  $\Delta P_0 + LAP$ . So, we can convert the equation (Eq. 7) to another equation:

$$(\Delta P + LAP) = (\Delta P_0 + LAP) \times e^{-t/\tau} \quad (\text{Eq. 8})$$

We can give some absolute numbers for  $\Delta P$  and  $\Delta P_0$ , such that  $\Delta P = 0$  mmHg and  $\Delta P_0 = 64$  mmHg or  $\Delta P_0 = 36$  mmHg (Fig. 1). So we can rewrite the equations as:

$$(0 + LAP) = (64 + LAP) \times e^{-t_1/\tau} \quad (\text{Eq. 9})$$

$$(0 + LAP) = (36 + LAP) \times e^{-t_2/\tau} \quad (\text{Eq. 10})$$

Natural logarithm of each side of each equation gives two other equations:

$$\ln(LAP) = \ln(64 + LAP) - t_1/\tau \quad (\text{Eq. 11})$$

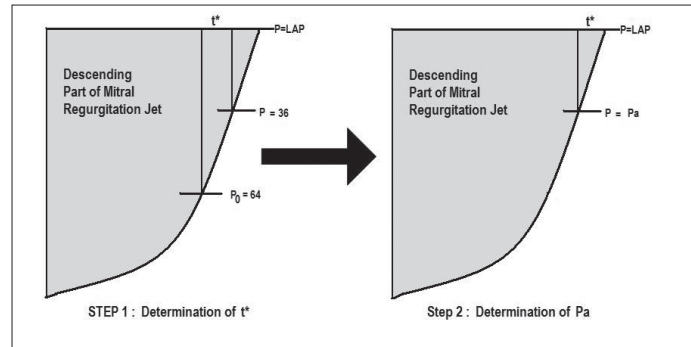


Figure 1. The illustration of determining  $t^*$  and  $P_a$

$$\ln(LAP) = \ln(36 + LAP) - t_2/\tau \quad (\text{Eq. 12})$$

We can convert these equations into two other equations:

$$t_1/\tau = \ln(64 + LAP) - \ln(LAP) \quad (\text{Eq. 13})$$

$$t_2/\tau = \ln(36 + LAP) - \ln(LAP) \quad (\text{Eq. 14})$$

If we divide right side of the Eq. 13 with the right side of the Eq. 14 and left side with left side, we obtain another equation:

$$t_1/t_2 = [\ln(64 + LAP) - \ln(LAP)] / [\ln(36 + LAP) - \ln(LAP)] \quad (\text{Eq. 15})$$

It is seen that  $t_1/t_2$  is a function of  $LAP$  alone. This hypothesis was tested by a clinical study and it was confirmed that this principle is valid (4).

There is another support for the validity of the Eq. 8. It was proposed by Chen et al. (5) that  $\tau$  can be measured from the MR jet. Their method was based on the measurement of the time duration from 3 m/s velocity to 1 m/s velocity of MR jet on the descending part. So they used the  $\Delta P$  as 36 mmHg and 4 mmHg. Then:

$$(LAP + 4) = (LAP + 36) \times e^{-t/\tau} \quad (\text{Eq. 16})$$

According to their proposal, the  $t$  should be equal to  $\tau$ , then:

$$(LAP + 4) = (LAP + 36) \times e^{-\tau/\tau} \quad (\text{Eq. 17})$$

$$(LAP + 4) = (LAP + 36) \times e^{-1} \quad (\text{Eq. 18})$$

$$(LAP + 4) = (LAP + 36) \times 0,37 \quad (\text{Eq. 19})$$

According to this equation,  $LAP$  should be 14.8 mmHg to validate this method. However, they have reported that they had assumed  $LAP$  as 10 mmHg. On the other hand, they also confessed that this assumption has led to underestimation of the  $\tau$ . Although they have not mentioned, the underestimation of  $\tau$  may be explained by this assumption. Never the less, this assumption may take us to another position. We can easily measure the time interval from 3 m/s to 1 m/s on the MR jet (Fig. 1, step 1). Let's define this interval as  $t^*$ . Afterwards, let's find the point on the descending part of the jet, which is  $t^*$  away from the end of the jet. Let's define this point as  $P_a$  (Fig. 1, step 2). Then:

$$(0 + LAP) = (P_a + LAP) \times e^{-t^*/\tau} \quad (\text{Eq. 20})$$

$$(4 + LAP) = (36 + LAP) \times e^{-t^*/\tau} \quad (\text{Eq. 21})$$

If we divide one side of the Eq. 22 with same side of the Eq. 23, then:

$$LAP/(4 + LAP) = (P_a + LAP) / (36 + LAP) \quad (\text{Eq. 22})$$

Then,

$$LAP = (4 \times P_a) / (32 - P_a) \quad (\text{Eq. 23})$$

It is seen from the equation that  $P_a$  is a function of  $LAP$  and gives information about the  $LAP$ .

We can convert Eq. 8 to another equation:

$$e^{-t^*/\tau} = (36 + LAP) / (64 + LAP) \quad (\text{Eq. 24})$$

Natural logarithm of each side of the equation is:

$$-t^*/\tau = \ln[(36 + LAP) / (64 + LAP)] \quad (\text{Eq. 25})$$

$$t^*/\tau = \ln[(64 + LAP) / (36 + LAP)] \quad (\text{Eq. 26})$$

If we substitute  $LAP$  with the one in Eq. 23, then:

$$t^*/\tau = \ln\left\{\frac{64 + \left(\frac{4 \times P_a}{32 - P_a}\right)}{\left(36 + \left(\frac{4 \times P_a}{32 - P_a}\right)\right)}\right\} \quad (\text{Eq. 27})$$

So we can also conclude that,  $t^*/\tau$  is a function of Pa. Therefore, if we can accurately point the Pa, we will obtain information about two important parameters of diastolic function: LAP and  $\tau$ .

In fact, it is very difficult to use these equations for exactly predicting the parameters because they are very complex. However, after proving the validity of these hypotheses, the devices can automatically calculate the dependent parameters, resulting in more efficient use of Doppler echocardiography.

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## Myxomanın arteri

### *The myxoma's artery*

Sayın Editör,

Kardiyak miksomalar en sık rastlanan kardiyak neoplazilerdir. Tüm kardiyak neoplazilerin %30 ile 50'sini oluştururlar. Anjiyografik olarak kanıtlanmış neovaskülarizasyon %30 ile 40'ında görülmektedir. Neovaskülarizasyon sol sirkümfleks veya sağ koroner arterden eşit sıklıkla köken alır (1).

Miksomanın besleyici arterine yazarların (2-4) ve derginizin gösterdiği ilgi bizleri memnun etmektedir. Ekibimiz de miksomanın arterinin görüntülendiği bir olgu nedeniyle bu konu ile ilgilenmektedir (5) ve katkıda bulunmayı amaçlamaktadır.

Bir koroner arter ile bir kalp boşluğu arasında bulunan fistüller genelde doğuştan olup anjiyografi için refere edilen hastaların

%0,17'sinde mevcuttur. Bir koroner arter ile bir kalp boşluğu arasında akkiz fistüle nadiren rastlanır. Aterosklerotik koroner arter hastalığı, mitral stenozla birlikte sol atriyal trombus varlığı, rezeke edilmemiş miksoma varlığında fistül rapor edilmiş olup bir atriyal miksoma rezeksiyonu sonrası sol atriyum içine fistül oluşumu daha nadirdir. Bilindiği üzere, miksoma tanısı alan her hastada koroner anjiyografi rutin olarak uygulanmamaktadır. Genelde 40 yaş altı erkekler ve 45 yaş altı kadınlarda ekokardiyografi ile tanı kesinleştirilip cerrahi tedaviye yönelinir. Anjiyografi uygulanmaz. Miksomalar, ağırlıklı olarak atriyal septumdan kaynaklanır ve cerrahi tedavisinde miksomanın pedikülü ile birlikte yaklaşık 1 cm çapında atriyal septum da rezeke edilir. Septumda oluşan defekt, sonrasında onarılır. Roth ve arkadaşlarının (1) çalışması, sol atriyumdaki miksoma rezeksiyonundan yıllar sonra bile arteriyatriyal fistül gelişebileceğini göstermiştir. Bu makale, bizim kanaatimize göre, yukarıdaki cerrahi yöntemin gözden geçirilmesi gerekliliğini ortaya koymaktadır. Miksomanın besleyici arteri anjiyografik olarak görüntülense de görüntülenmese de, cerrahi sırasında bu arter bağlansa da bağlanmasa da miksomanın sapının etrafındaki dokunun (atriyal septum, atriyal duvar) –eğer uygunsa- radyofrekans ablasyon yöntemi ile koterize edilmesi gerekliliği kanısını oluşturmaktadır. Diğer cerrahi koterler, kullanımları halinde aritmojenik odak teşkil edebileceği için, radyofrekans ablasyon uygulamasının tercih edilmesi gerektiğini düşünmekteyiz (5).

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